

AFRL-RH-WP-JA-2009-0001

Assessment of Muscle Fatigue from TF Distributions of SEMG Signals

C. Potes
R. von Borries
C. Jacques Miosso
J.H. Pierluissi
Department of Electrical and Computer Engineering
The University of Texas at El Paso
El Paso TX 79968

June 2008

Interim Report for September 2006 to June 2008

Approved for public release; distribution is unlimited.

Air Force Research Laboratory
711th Human Performance Wing
Human Effectiveness Directorate
Biosciences and Protection Division
Biomechanics Branch
Wright-Patterson AFB OH 45433-7947

NOTICE AND SIGNATURE PAGE

Using Government drawings, specifications, or other data included in this document for any purpose other than Government procurement does not in any way obligate the U.S. Government. The fact that the Government formulated or supplied the drawings, specifications, or other data does not license the holder or any other person or corporation; or convey any rights or permission to manufacture, use, or sell any patented invention that may relate to them.

This report was cleared for public release by the 88th ABW Air Base Wing Public Affairs Office and is available to the general public, including foreign nationals. Copies may be obtained from the Defense Technical Information Center (DTIC) (http://www.dtic.mil).

THIS REPORT HAS BEEN REVIEWED AND IS APPROVED FOR PUBLICATION IN ACCORDANCE WITH ASSIGNED DISTRIBUTION STATEMENT.

AFRL-RH-WP-JA-2009-0001

//SIGNED//	//SIGNED//		
Nathan Wright, Work Unit Manager	Mark M. Hoffman, Deputy		
Biomechanics Branch	Biosciences and Protection Division		
	Human Effectiveness Directorate		
	711 th Human Performance Wing		
	Air Force Research Laboratory		

This report is published in the interest of scientific and technical information exchange, and its publication does not constitute the Government's approval or disapproval of its ideas or findings.

DEDORT DO	Form Approved		
REPORT DO	OMB No. 0704-0188		
data needed, and completing and reviewing this collection this burden to Department of Defense, Washington Heads	estimated to average 1 hour per response, including the time for reviewing ins of information. Send comments regarding this burden estimate or any other a quarters Services, Directorate for Information Operations and Reports (0704-00) any other provision of law, no person shall be subject to any penalty for failing YOUR FORM TO THE ABOVE ADDRESS.	aspect of this collection of information, including suggestions for reducing 188), 1215 Jefferson Davis Highway, Suite 1204, Arlington, VA 22202-	
1. REPORT DATE (DD-MM-YYYY)	2. REPORT TYPE	3. DATES COVERED (From - To)	
June 2008	Interim Report	September 2006 – June 2008	
4. TITLE AND SUBTITLE	5a. CONTRACT NUMBER		
	FA8650-06-1-6748		
Assessment of Muscle Fatigue f	5b. GRANT NUMBER		
		5c. PROGRAM ELEMENT NUMBER	
6. AUTHOR(S)		5d. PROJECT NUMBER	
o. Ad Hok(3)	7184		
C. Potes, R. von Borries, C. Jac	5e. TASK NUMBER		
1, 1, 1, 1, 1, 1, 1, 1, 1, 1, 1, 1		02	
		5f. WORK UNIT NUMBER	
7 DEDECOMING ODGANIZATION NAME	71840219		
7. PERFORMING ORGANIZATION NAME	8. PERFORMING ORGANIZATION REPORT NUMBER		
Department of Electrical and Co	omputer Engineering		
The University of Texas at El P			
El Paso TX 79968			
9. SPONSORING / MONITORING AGENC	, ,	10. SPONSOR/MONITOR'S ACRONYM(S)	
Air Force Materiel Comman		711 HPW/RHPA	
Air Force Research Laborato			
711 th Human Performance W	-		
Human Effectiveness Director	11. SPONSOR/MONITOR'S REPORT		
Biosciences and Protection I	NUMBER(S)		
Biomechanics Branch	` '		
Wright-Patterson AFB OH 4	AFRL-RH-WP-JA-2009-0001		
12. DISTRIBUTION / AVAILABILITY STAT	EMENT		
Approved for public release;	distribution is unlimited.		
13. SUPPLEMENTARY NOTES			
88 ABW/PA cleared on 25M	Iar08, WPAFB 08-2108.		
14. ABSTRACT			
In this paper we present a comp	arison of four techniques used to build a tin	ne-frequency (TF) distribution of surface	
electromyographic signal (SEM	G) signals, namely spectrogram, Wigner-V	ille, Choi-Williams and smoothed	

pseudo Wigner-Ville.

15. SUBJECT TERMS							
16. SECURITY CLASSIFICATION OF:		17. LIMITATION	18. NUMBER	19a. NAME OF RESPONSIBLE PERSON			
			OF ABSTRACT	OF PAGES	Nathan Wright		
a. REPORT	b. ABSTRACT	c. THIS PAGE		5	19b. TELEPHONE NUMBER (include area		
			SAR		code)		
T T	IT	II	Di III		l NA		

THIS PAGE IS INTENTIONALLY LEFT BLANK

ASSESSMENT OF MUSCLE FATIGUE FROM TF DISTRIBUTIONS OF SEMG SIGNALS

C. Potes, R. von Borries, C. Jacques Miosso, and J. H. Pierluissi

Department of Electrical & Computer Engineering
The University of Texas at El Paso, El Paso, Texas 79968, USA
Email: cmpotes@miners.utep.edu

ABSTRACT

Assessment of muscle fatigue involves the creation of indices based on the estimation of variables such as the instantaneous frequency (IF) and the instantaneous amplitude (IA), which can be estimated from a time-frequency (TF) distribution of a surface electromyographic signal (SEMG). Since during muscle fatigue there is a decrease of the IF and an increase of the IA, slopes from these parameters can be computed and used as indices to measure muscle fatigue. In this paper we present a comparison of four techniques used to build a TF distribution of SEMG signals, namely spectrogram, Wigner-Ville, Choi-Williams and smoothed pseudo Wigner-Ville. SEMG signals were recorded from thirty normal human subjects under specific physical routines to measure muscle fatigue, and TF distributions were computed for all the acquired signals. In order to confirm muscle fatigue, the computed indices were then correlated to the perceived discomfort levels reported by the subjects. Results show that although the spectrogram and smoothed pseudo Wigner-Ville have to overcome problems such as sizes of the time and frequency windows and cross terms, these two distributions provide equivalent slopes and valid indices of muscle fatigue for SEMG signals with low to medium nonstationarity.

ESTIMATION OF FREQUENCY AND AMPLITUDE FROM TF DISTRIBUTIONS

Muscle fatigue can be assessed from IF and IA of SEMG signals [1], [2], [3]. The approaches in the assessment of muscle fatigue have been restricted to the nature of the measured SEMG signal. If the SEMG signal is recorded during isometric constant force contractions, it is considered wide-sense stationary over time intervals lasting from 1 to 2 seconds [4]. Otherwise, if the SEMG signal is recorded during dynamic contractions, the signal is considered nonstationary [1], [4]. The spectrogram has been used to estimate the IF of SEMG signals with isometric contractions. In the case of nonstationary SEMG signals, not only the spectrogram but also other Cohen's class TF distributions, such as the Choi-Williams distribution (CWD) and the smoothed pseudo Wigner-Ville distribution (SPWVD) have been used to estimate the IF [1], [2]. However, in the assessment of muscle fatigue, we should analyze not only the IF but also the IA of the SEMG signal. The root mean square and the mean absolute value have been employed in the estimation of the IA of stationary and nonstationary SEMG signals [4], [6]. In this paper we compute both IF and IA from the spectrogram and the SPWVD – IF from the first order moment of the frequency distribution at a point in time and IA from the square root of the smoothed time marginal.

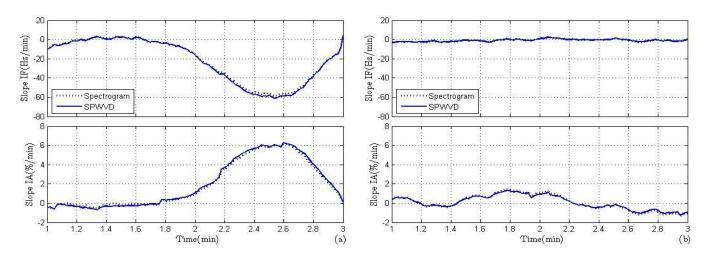
The implemented techniques for computing the TF distributions were evaluated based on aspects that are desired in SEMG analysis such as positivity, time and frequency marginals, and finite support. Also, an important desired characteristic is the suppression of cross terms since they lead to wrong estimates of the IF. Among the evaluated techniques, the spectrogram is computationally fast and the only always with a positive distribution. However, it shows a time-frequency localization trade-off and it does not hold the time and frequency marginals or the finite support [3], [4], [5]. On the other hand, the Wigner-Ville distribution (WVD) holds the time and frequency marginals and finite time support, but it is non-positive and leads to cross-terms when applied to multicomponent signals (as SEMG signals) [3], [4]. The

CWD and the SPWVD are obtained by convolving the WVD with different kernels, which make the WVD more local and reduce cross terms. The CWD holds time and frequency marginals and localization, but it is still not always positive, it has no time and frequency support, and its kernel depends on the choice of a critical parameter which has to be adapted for each signal [1]. Finally, the SPWVD can provide adequate estimates of the IF, but it does not hold the time and frequency marginals, finite support, and also leads to time-frequency localization trade-off.

EVALUATION OF MUSCLE FATIGUE

The SEMG signals used in this experiment were recorded from 30 normal human subjects who performed a 70% maximum voluntary contraction (MVC). This exertion was held until the subject could no longer maintain a 70% MVC or up to three minutes. The IF and the IA of the recorded signals were then estimated using the spectrogram, CWD, and SPWVD. However, since the CWD provided negative instantaneous frequencies, the measured IF from the CWD was not included in the evaluation of muscle fatigue. By employing a joint analysis of the spectrum and the amplitude (JASA) [6], slopes from the estimated IF and the IA were computed using a linear regression model and were calculated for oneminute intervals every one-second. Indices of muscle fatigue, recovery, increase force, and decrease force were then extracted from the slopes, and indices of muscle fatigue were correlated to the perceived discomfort levels reported by the subjects. The results for 2 out of 30 subjects are shown in Fig. 1. Figure 1(a) shows that the slopes for subject 1 at hour 6 reached a minimum of -60 Hz/min and a corresponding maximum of 6 %/min (percentage of the total amplitude), indicating the development of muscle fatigue. This matches the reported discomfort level. Subject 1 selected pain and severe hot spots in head, neck, shoulders, and back at the end of hour 6. Figure 1(b) shows small changes in the IF and IA for subject 2 at hour 1, indicating that fatigue was not present. This also matches the reported discomfort level. Subject 2 selected no discomfort and no hot spots in head, neck, shoulders and back at the end of hour 1.

Although the size of the time and frequency windows and the suppression of cross terms are important factors in the estimation of IF and IA, equivalent indices of muscle fatigue can be obtained from the spectrogram and the SPWVD, as indicated in the analysis of an extensive set of SEMG signals with low to medium nonstationarity.



Research supported by AFRL – FA8650-06-1-6748

BIBLIOGRAPHY

- [1] S. Karlsson, J. Yu, and M. Akay. Time-frequency analysis of myoelectric signals during dynamic contractions: A compartive study. *IEEE Transactions on Biomedical Engineering*, 47:228–238, 2000.
- [2] P. Bonato, G. Giagliati, and M. Knaflitz. Analysis of myoelectric signals recorded during dynamic contractions. *IEEE Engineering in medicine and Biology*, 15:102–111, 1996.
- [3] L. Cohen. Time-Frequency Analysis. Prentice Hall Professional, Upper Saddle River, NJ, 1995.
- [4] R. Merletti and P. A. Parker, editors. *Electromyography: Physiology, Engineering, and Noninvasive Applications*. John Wiley & Sons, Hoboken, NJ, 2004.
- [5] A. Papandreou-Suppappola, editor. *Applications in Time-Frequency Signal Processing*. CRC Press, Boca Raton, FL, 2003.
- [6] A. Luttmann, M. Jäger, and W. Laurig. Electromyographical indication of muscular fatigue in occupational field studies. *International Journal of Industrial Ergonomics*, 25:645–660, 2000.